

## Membrane Potentials and Intracellular Cl<sup>-</sup> Activity of Toad Skin Epithelium in Relation to Activation and Deactivation of the Transepithelial Cl<sup>-</sup> Conductance

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**Summary.** The potential dependence of unidirectional <sup>36</sup>Cl fluxes through toad skin revealed activation of a conductive pathway in the physiological region of transepithelial potentials. Activation of the conductance was dependent on the presence of Cl<sup>-</sup> or Br<sup>-</sup> in the external bathing solution, but was independent of whether the external bath was NaCl-Ringer's, NaCl-Ringer's with amiloride, KCl-Ringer's or choline Cl-Ringer's. To partition the routes of the conductive Cl<sup>-</sup> ion flow, we measured in the isolated epithelium with double-barrelled microelectrodes apical membrane potential,  $V_a$ , and intracellular Cl<sup>-</sup> activity,  $a_{Cl}^i$ , of the principal cells identified by differential interference contrast microscopy. Under short-circuit conditions,  $I_{sc} = 27.0 \pm 2.0 \mu A/cm^2$ , with NaCl-Ringer's bathing both surfaces,  $V_a$  was  $-67.9 \pm 3.8$  mV (mean  $\pm$  SE,  $n = 24$ , six preparations) and  $a_{Cl}^i$  was  $18.0 \pm 0.9$  mM in skins from animals adapted to distilled water. Both  $V_a$  and  $a_{Cl}^i$  were found to be positively correlated with  $I_{sc}$  ( $r = 0.66$  and  $r = 0.70$ , respectively). In eight epithelia from animals adapted to dry milieu/tap water  $V_a$  and  $a_{Cl}^i$  were measured with KCl Ringer's on the outside during activation and deactivation of the transepithelial Cl<sup>-</sup> conductance ( $G_{Cl}$ ) by voltage clamping the transepithelial potential ( $V$ ) at 40 mV (mucosa positive) and  $-100$  mV. At  $V = 40$  mV; i.e. when  $G_{Cl}$  was deactivated,  $V_a$  was  $-70.1 \pm 5.0$  mV ( $n = 15$ , eight preparations) and  $a_{Cl}^i$  was  $40.0 \pm 3.8$  mM. The fractional apical membrane resistance ( $fR_a$ ) was  $0.69 \pm 0.03$ . Clamping to  $V = -100$  mV led to an instantaneous change of  $V_a$  to  $31.3 \pm 5.6$  mV (cell interior positive with respect to the mucosal bath), whereas neither  $a_{Cl}^i$  nor  $fR_a$  changed significantly within a 2 to 5-min period during which  $G_{Cl}$  increased by  $1.19 \pm 0.10$  mS/cm<sup>2</sup>. When  $V$  was stepped back to 40 mV,  $V_a$  instantaneously shifted to  $-67.8 \pm 3.9$  mV while  $a_{Cl}^i$  and  $fR_a$  remained constant during deactivation of  $G_{Cl}$ . Similar results were obtained in epithelia impaled from the serosal side. In 12 skins from animals adapted to either tap water or distilled water the density of mitochondria-rich ( $D_{MRC}$ ) cells was estimated and correlated with the Cl<sup>-</sup> current ( $I_{Cl}$ ) through the fully activated ( $V = -100$  mV) Cl<sup>-</sup> conductance. A highly significant correlation was revealed ( $r = -0.96$ ) with a slope of  $-2.6$  nA/m.r. (mitochondria-rich cell and an I-axis intercept not significantly different from zero). In summary, the voltage-dependent Cl<sup>-</sup> currents were not reflected in  $fR_a$  and  $a_{Cl}^i$  of the principal cells but showed a correlation with the m.r. cell density. We conclude that the principal cells do not contribute significantly to the voltage-dependent Cl<sup>-</sup> conductance.

**Key Words** toad skin epithelium · voltage-clamp currents · membrane potential · intracellular Cl<sup>-</sup> activity · voltage-dependent Cl<sup>-</sup> conductance · mitochondria-rich cells

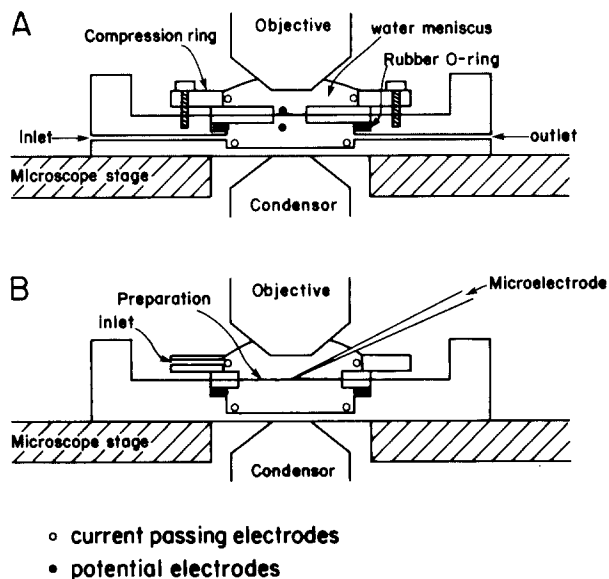
### Introduction

Passive transepithelial Cl<sup>-</sup> fluxes of toad (*Bufo bufo*) skin exhibit a complex voltage-dependence owing to a gated Cl<sup>-</sup> permeability that is turned on over the range of physiological potentials (mucosa negative) and turned off at potentials above 0 mV. As a result, the steady-state conductive Cl<sup>-</sup> ion flow is large only when its electric driving force is inwardly directed, whereas the net flux of Cl<sup>-</sup> becomes virtually zero when the driving force is reversed (Larsen & Kristensen, 1978; Larsen & Rasmussen, 1982).

As the magnitude of passive Cl<sup>-</sup> fluxes in the short-circuited frog skin decreases when the active Na<sup>+</sup> flux is reduced (Macey & Meyers, 1963; Candia, 1978; Kristensen, 1978; Ques-von Petery et al., 1978), the Cl<sup>-</sup> permeability was suggested to reside in a major Na<sup>+</sup>-transporting compartment, i.e. the principal cells<sup>1</sup> of the epithelium. However, results published recently by others are difficult to reconcile with the passage of large dissipative Cl<sup>-</sup> fluxes through these cells. For example, under short-circuit conditions a low Cl<sup>-</sup> permeability of the outer epithelial barrier (Nagel, 1977; Ferreira & Ferreira, 1981; Nagel et al., 1981; Stoddard & Helman, 1982; Giraldez & Ferreira, 1984; Biber et al., 1985) and an intracellular Cl<sup>-</sup> activity far above equilibrium (Rick et al., 1978; Nagel et al., 1981; Giraldez & Ferreira, 1984; Harvey & Kernan, 1984; Biber et al., 1985) have been reported. Furthermore, Voûte and Meier (1978), Kristensen (1981) and Katz and Larsen (1984) presented evidence that the trans-

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<sup>1</sup> Principal cells denotes the major population of epithelial cells located from the stratum germinativum to the stratum granulosum, excluding the m.r. cells.



**Fig. 1.** Experimental chamber for microelectrode measurements in identified cells of isolated epithelia. Panels A and B show perpendicular cross-sections illustrating the rectangular positions of electrodes, perfusion tubes, and the exposed epithelial area. The Figure is not drawn to scale

epithelial Cl<sup>-</sup> pathway in the frog or toad skin is localized to the mitochondria rich (m.r.) cells. Because these cells do not take part in the functional syncytium made up by the more numerous principal cells (Rick et al., 1978), the dependence of the Cl<sup>-</sup> fluxes on the active Na<sup>+</sup> flux suggests that at least a small component of the active Na<sup>+</sup> flux passes the m.r. cells. This view is supported by the finding that excretion of the vital dye, methylene blue, by the m.r. cells is inhibited by amiloride and ouabain (Ehrenfeld et al., 1976), which are specific blockers of active Na<sup>+</sup> transport in high-resistance epithelia. Also it is in agreement with the finding that the Na<sup>+</sup> gain by m.r. cells following ouabain treatment of frog skin was partially prevented by exposure of the outer border of the skin to amiloride (Rick et al., 1978).

In the present study we investigated the conductive Cl<sup>-</sup> permeability of the principal cells of toad skin. This was done by measurements of membrane potentials and the intracellular Cl<sup>-</sup> activity of these cells in response to voltage activation and deactivation of the transepithelial Cl<sup>-</sup> conductance. We also determined the relationship between the density of the mitochondria-rich cells, and the fully activated potential-dependent Cl<sup>-</sup> conductance. Thus, the experiments to be presented extend previous tracer flux (Ferreira & Ferreira, 1981; Stoddard & Helman, 1982) and microelectrode (Nagel et al., 1981; Harvey & Kernan, 1984; Biber et al., 1985) studies of the short-circuited frog skin by tak-

ing in account that at  $V = 0$  mV the conductive Cl<sup>-</sup> permeability is very low, but that the Cl<sup>-</sup> conductance reversibly can be turned fully on by clamping the tissue at  $V \leq -80$  mV.

Part of this study have been published elsewhere (Willumsen & Larsen, 1984, 1985a,b).

## Materials and Methods

### PREPARATION

The epidermis of the belly skin, isolated in the intermolt period, was obtained from the common European toad (*Bufo bufo*). The majority of experiments to be reported were carried out with animals kept on filter paper with free access to tap water and given mealworms *ad libitum*, i.e. under conditions mimicking the natural habitat of this terrestrial species.

In contrast to animals kept under the above conditions, skin of animals kept in distilled water generally exhibit larger, more variable short-circuit currents. Thus, for the initial studies on membrane potentials and intracellular Cl<sup>-</sup> activities, we used animals kept in distilled water (8 to 12 days), to compare our measurements with those reported in the literature from frog skins generating similar large and variable short-circuit currents.

The epithelium was isolated by exposing the serosal side of the skin to a 0.25 mg/ml collagenase solution (103586, Boehringer Mannheim GmbH) for 2 to 3 hr. After this treatment the intact epithelium was removed from the partly digested corium and stored at 5°C in NaCl-Ringer's containing 5 mM acetate.

### EXPERIMENTAL CHAMBER

The isolated epithelium was mounted in a mini Ussing-chamber with a slit-shaped exposed area of  $2 \times 5$  mm (Fig. 1). The serosal and the mucosal half-chambers, that could be perfused continuously, contained a pair of Ag/AgCl electrodes for potential recording and current passing, respectively. These were connected to a voltage-clamp circuit providing fast (msec) voltage clamping of the preparation between  $-200$  and  $+200$  mV. The chamber was placed directly on a microscope stage, and the impalements were visually inspected at  $400\times$  magnification by differential interference contrast (DIC, Nomarski) microscopy employing a Zeiss 40/0.75 water immersion objective with a working distance of 1.6 mm.

### RINGER'S SOLUTIONS

The composition of the employed Ringer's solution was:

NaCl-Ringer's (mM): 114.4 Na<sup>+</sup>, 2.4 K<sup>+</sup>, 1.0 Ca<sup>2+</sup>, 116.4 Cl<sup>-</sup>, 2.4 HCO<sub>3</sub><sup>-</sup>, pH = 8.2 following bubbling with atmospheric air. To the NaCl-Ringer's bathing the serosal side was added 5 mM Na-acetate.

KCl-Ringer's: Na<sup>+</sup> substituted by K<sup>+</sup>. Otherwise identical to NaCl-Ringer's.

Na-gluconate-Ringer's: Cl<sup>-</sup> substituted by gluconate. Otherwise identical to NaCl-Ringer's.

### MICROELECTRODES

Double-barrelled Cl<sup>-</sup>-selective microelectrodes were constructed according to the technique of Zeuthen et al. (1974) from

1.2 mm OD glass capillary (Corning 120F) for the reference barrel and 1.8 mm OD glass capillary (Jencons) for the ion-selective barrel. The nitric acid-washed capillaries were glued together with an epoxy glue (Araldit) heated and twisted 360°, and pulled on a horizontal puller (Narishige, model PD-5). The tip diameter of the electrode was less than 1 μm. The ion-selective barrel was silanized (dichlorodimethylsilane) for 5 to 10 sec and heated for 1 hr at 100°C before filling the tip with Cl<sup>-</sup> ion exchanger (Corning 477913). Finally, the ion-selective barrel was backfilled with 0.5 or 2 M KCl. The reference barrel was backfilled with either 0.5 M Na<sub>2</sub>SO<sub>4</sub> or 0.5 M KCl, or the tip was filled with 0.5 M Na<sub>2</sub>SO<sub>4</sub> whereas the stem of the electrode was filled with 2 M KCl. The estimated Cl<sup>-</sup> activities were independent of the electrolyte composition of the reference barrel, indicating that leakage of Cl<sup>-</sup> from the reference barrel was insignificant. Heating of the electrode was found to impair the selectivity and slow the response time of the ion exchanger. Therefore, air bubbles, if present, were removed by thin glass filaments. When filled with 2 M KCl, the resistance of the reference barrel was 30 to 100 Mohm. The electrodes were calibrated in KCl solutions of either variable (0.01, 0.03 and 0.1 M KCl) or constant (0.01 M KCl + 0.09 M Na-gluconate, 0.03 M KCl + 0.07 M Na-gluconate and 0.1 M KCl) ionic strength. In both cases, the sensitivity (*S*) ranged from 50 to 59 mV per decalog Cl<sup>-</sup> activity, with  $S = 57.4 \pm 0.5$  mV/decalog for 16 randomly selected electrodes. The HCO<sub>3</sub><sup>-</sup>/Cl<sup>-</sup> selectivity coefficient was  $0.11 \pm 0.01$  ( $n = 16$ ). As a rule, the electrode was calibrated before as well as after use, and we detected no change of its sensitivity following the impalements, whether the electrode tip was broken or intact. Tip potentials (defined as the difference in reference electrode signal between isosmotic solutions of NaCl and KCl) ranged from 0 to 15 mV, but electrodes with tip potentials greater than 5 mV were discarded. The response time of the electrodes was less than 2 sec. The two barrels were connected to a high-impedance preamplifier by a pair of silver wires. The signal of the reference barrel was electronically subtracted from the signal of the ion-selective barrel, and the output together with the signal of the reference barrel and the voltage-clamp current were continuously recorded on a multi-channel chart recorder (Watanabe MC-611). The intracellular Cl<sup>-</sup> activity was calculated by:

$$a_{\text{Cl}^-}^i = a_{\text{Cl}^-}^o \cdot 10^{\Delta E/S}$$

where  $a_{\text{Cl}^-}^o$  is the Cl<sup>-</sup> activity of the outside bathing Ringer's,  $\Delta E$  is the differential electrode signal with reference to the outer bath, and *S* is the sensitivity.

### Impalements

Due to the position of the microscope objective, the electrode was advanced at an angle of 25 to 30° relative to the epithelial surface. The electrode was advanced by a hydraulic motorized step micromanipulator (David Kopf Instruments, Model 1207B) with a minimal step length of 0.25 μm.

Often, the initially recorded potential decayed to a much smaller value within a few seconds indicating that the membrane was damaged by the penetration. Penetration of the outermost tough keratinized stratum corneum layer may give rise also to artifactual potentials of the nondecaying type (Nelson et al., 1978). Carefully selected criteria for acceptable impalements are therefore mandatory. The criteria were defined according mainly to Armstrong and Garcia-Diaz (1981) and Zeuthen (1984):

1. Visually the electrode tip should be seen to be localized

within a principal cell (a granulosum or, in some experiments, a germinativum cell). However, due to the distortion of the tissue we could not always evaluate whether the cell impaled from the outside belonged to the outermost living epithelial cell layer or to a more deeply located layer.

2. The potential changes should be sudden.

3. During a steady state, the electrode signals should be time invariant. Following perturbations of the transepithelial potential, the electrode signals should return to their initial values when *V* was stepped back and the initial steady-state re-established.

4. Following impalement, the electrode-resistance ( $R_e$ ) should be comparable to  $R_e$  measured outside the epithelium. Furthermore,  $R_e$  should be identical before and after the impalement indicating that the tip is not damaged or blocked.

5. The voltage divider ratio should suddenly increase indicating that a major resistance barrier was passed.

Due to the specific properties of the tissue, another criterion was to be fulfilled for epithelia exposed to NaCl-Ringer's outside: Application of amiloride to the outside bath should result in a hyperpolarization of the reference electrode potential (Nagel, 1976; Helman & Fisher, 1977).

### DETERMINATION OF THE RELATIONSHIP BETWEEN $I_{\text{Cl}^-}$ AND $D_{\text{MRC}}$

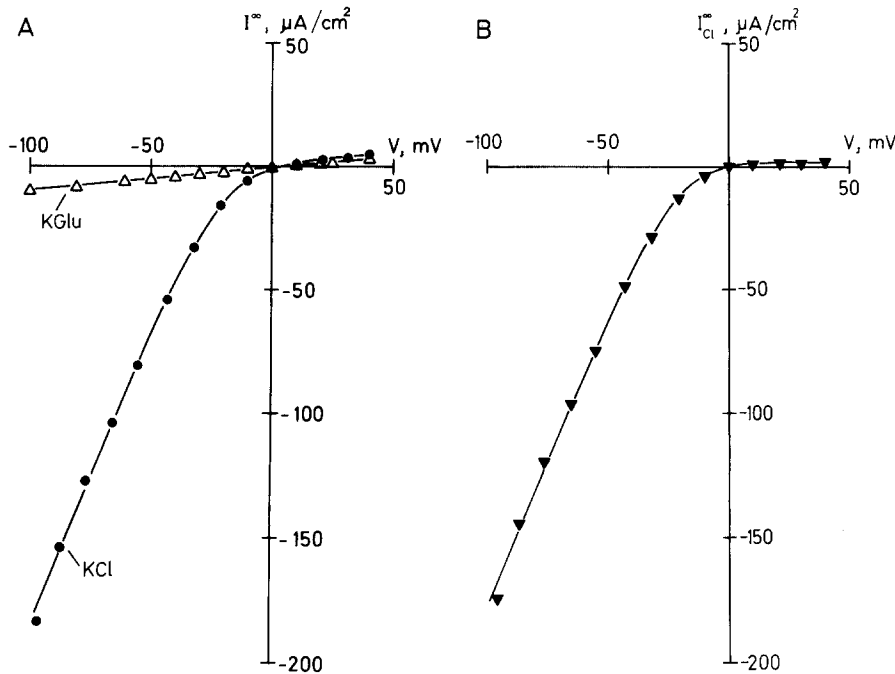
To estimate the density of the m.r. cells we employed the silver-staining technique (Rudneff, 1865; Whitear, 1975). The outside of the skin was rinsed with distilled water. Following 4-min exposure to 0.25% AgNO<sub>3</sub>, the surface was rinsed again with distilled water and exposed to daylight or artificial light for a few minutes. Following this treatment, the m.r. cells were clearly visible. The density was determined either by direct microscopic counting of m.r. cells in randomly selected areas or by counting within skin areas of 0.5 mm<sup>2</sup> from photographs at 300× magnification. The Cl<sup>-</sup> current was determined as the difference between the steady-state voltage-clamp current measured at *V* = -100 mV (mucosal solution negative) and the leak-current, i.e. the voltage-clamp current measured initially after stepping *V* from 40 to -100 mV.

### MEASUREMENTS OF UNIDIRECTIONAL Cl<sup>-</sup> FLUXES

Influx and efflux of <sup>36</sup>Cl were measured in paired (whole) skins of the same toad mounted in Perspex® chambers with exposed areas of 7 cm<sup>2</sup> according to the method described by Katz and Larsen (1984). Briefly, the skin was bathed with NaCl-Ringer's on the inside and KCl-Ringer's on the outside, and clamped at the desired potential with automatic correction for the resistance between the potential bridges. The current and potential were continuously monitored by a dual pen-recorder and, in addition, the current was time-integrated and read when a sample of the "cold" solution was taken. Starting with 50 mV, each pair of skins was used for measurements of Cl<sup>-</sup> fluxes at usually three different clamping potentials. In 10 experiments, *V* was brought back to 50 mV after having finished the third period, and the measurements continued for a fourth period.

### SIGN CONVENTIONS

The transepithelial potential difference (*V*) is referenced as the potential of the mucosal bath ( $\psi_o$ ) minus the potential of the



**Fig. 2.** (A) Potential dependence of steady-state currents through toad skin exposed to either KCl Ringer's ( $\bullet$ ) or K-gluconate Ringer's ( $\Delta$ ) outside. Inside bath, NaCl-Ringer's. (B) Estimated  $I$ - $V$  relationship of the  $\text{Cl}^-$ -conductive pathway obtained as the difference between the two graphs shown in Fig. 2A.

serosal bath ( $\psi_o$ ),  $V = \psi_o - \psi_i$ . Intracellular potentials are referenced with respect to the bath from which the micropipette was advanced, i.e. from the apical bath,  $V_a = \psi_c - \psi_o$ , or from the serosal bath,  $V_b = \psi_c - \psi_i$ , where  $\psi_c$  is the potential of the micropipette with the tip positioned in a cell. Inward currents are defined positive.

## Results

### POTENTIAL DEPENDENCE OF TRANSEPIHELIAL CURRENTS

Figure 2A shows that with  $\text{Cl}^-$ -Ringer's outside, steady-state transepithelial currents were strongly rectified with large outward-going components for  $V < 0$  mV. The linear  $I/V$  relationship of the tissue with gluconate outside reflects a leakage conductance of less than  $100 \mu\text{S}/\text{cm}^2$ . The difference in the currents seen in the two graphs of Fig. 2A provides an estimate of the  $I_{\text{Cl}^-}$ - $V$  relationship of the preparation (Fig. 2B). The result indicates that the  $\text{Cl}^-$  ions are free to flow through the skin for  $V < 0$  mV, but not for  $V > 0$  mV. The same conclusion was obtained from  $\text{Cl}^-$  flux measurements in skins exposed to NaCl-Ringer's on the outside (Bruus et al., 1976).

Whereas the above method is fast, and can be applied to a single preparation, a detailed analysis of the conductive pathways requires the measurement of  $\text{Cl}^-$  influx ( $J_{\text{Cl}^-}^{\text{in}}$ ) and  $\text{Cl}^-$  outflux ( $J_{\text{Cl}^-}^{\text{out}}$ ) in paired belly skin halves from the same toad. The results are collected in Table 1, and the  $I$ - $V$  rela-

tionships are depicted in Fig. 3A. The conclusion to be drawn from the graphs shown in Fig. 3A is the same as that suggested by the indirect determination of the  $I_{\text{Cl}^-}$ - $V$  relationship shown in Fig. 2B. The  $I_{\text{Cl}^-}$ - $V$  relation intersects the  $I$ -axis at  $-1.81 \pm 0.31 \mu\text{A}/\text{cm}^2$  (mean  $\pm$  SE, significantly different from zero,  $P < 0.05\%$ ,  $n = 11$ ). Since the  $\text{Cl}^-$  ions are distributed in electrochemical equilibrium at  $V = 0$  mV, this result shows that the  $\text{Cl}^-$  ions are influenced by a driving force derived from a source other than the electrochemical potential difference of  $\text{Cl}^-$  between the inner and outer bathing solution. In Fig. 3B is shown the relation between the  $\text{Cl}^-$  current component and the total membrane current. The equation of the regression line is  $I = 1.05 I_{\text{Cl}^-} - 2.19 \mu\text{A}/\text{cm}^2$ , which is not significantly different from the line of identity, showing that the outward-clamping currents were carried by an inward flow of  $\text{Cl}^-$  ions. For  $V > 0$  mV, the  $\text{Cl}^-$  currents were too small to account for the clamping currents which, therefore, were carried by other ions, probably  $\text{K}^+$  (see Fig. 3A).

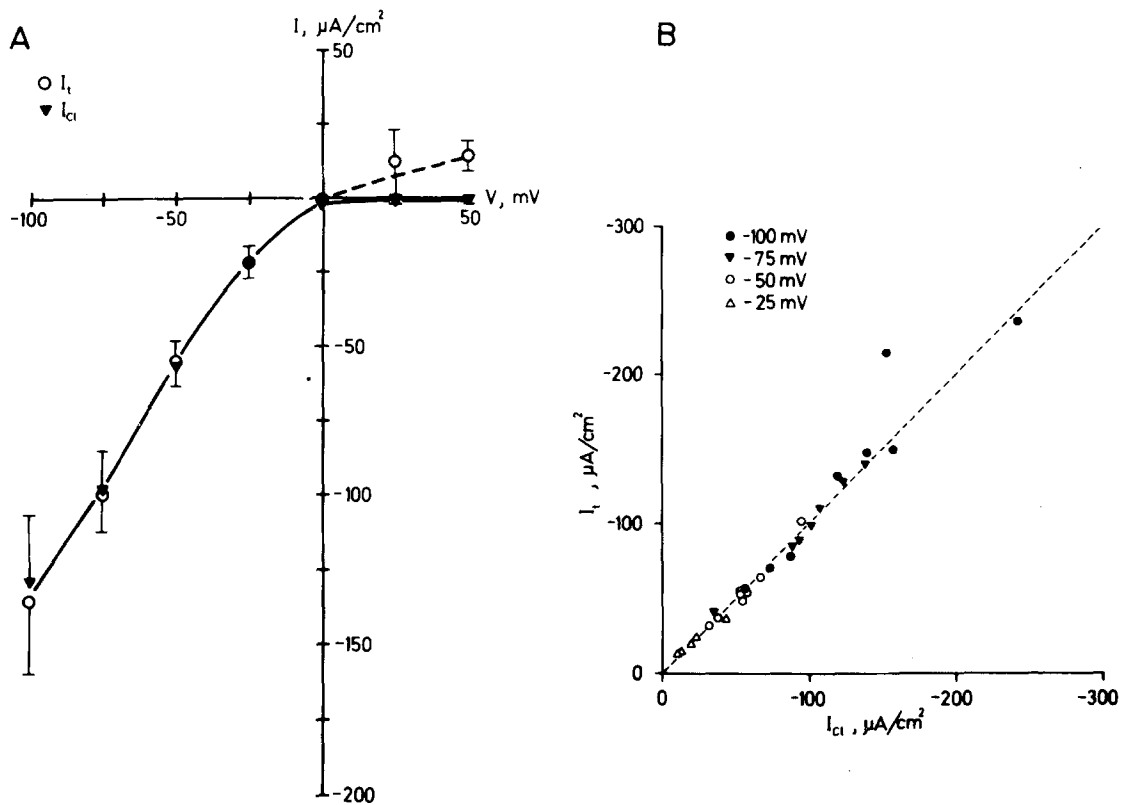
In ten sets of preparations, clamping at 50 mV finished the experimental protocol of 4-hr duration. In the final flux period,  $I_{\text{Cl}^-} = 0.48 \pm 1.96 \mu\text{A}/\text{cm}^2$ , as compared to  $I_{\text{Cl}^-} = -0.58 \pm 0.73 \mu\text{A}/\text{cm}^2$  for  $V = 50$  mV in the initial flux period following mounting of the preparations. Thus, the increase in  $\text{Cl}^-$  conductance was fully reversible. Furthermore, even in these experiments of long duration nonphysiological  $\text{Cl}^-$  leaks did not develop.

At  $V = 50$  mV, the total membrane current

**Table 1.** Unidirectional fluxes in toad skin exposed to NaCl-Ringer's on the inside and KCl-Ringer's on the outside<sup>a</sup>

V (mV)	J <sup>in</sup> (pmol/cm <sup>2</sup> sec)	J <sup>out</sup> (pmol/cm <sup>2</sup> sec)	J <sup>in</sup> /J <sup>out</sup>		I <sub>Cl</sub>	I <sub>tot</sub> (μA/cm <sup>2</sup> )	(n)
			Observed	Theoretical			
50	57 ± 17	51 ± 18	1.48 ± 0.25	0.14	-0.58 ± 0.73	14.2 ± 4.7	(13)
25	70 ± 25	58 ± 23	1.47 ± 0.34	0.37	-1.11 ± 0.99	12.2 ± 10	(5)
0	52 ± 7	33 ± 6	1.64 ± 0.12	1.00	-1.81 ± 0.31	-1.01 ± 0.21	(11)
-25	303 ± 71	76 ± 12	3.88 ± 0.33	2.67	-22.0 ± 5.8	-22.0 ± 4.2	(5)
-50	655 ± 78	67 ± 11	10.6 ± 1.0	7.14	-56 ± 6.7	-55.6 ± 7.5	(8)
-75	1055 ± 131	43 ± 5	24.4 ± 2.1	19.1	-98.0 ± 12	-99.0 ± 12	(7)
-100	1367 ± 222	29 ± 4.5	61.6 ± 13.3	51.0	-129 ± 21	-136 ± 23	(8)
50	128 ± 23	127 ± 30	1.27 ± 0.20	0.14	0.48 ± 1.96	30.1 ± 8.7	(10)

<sup>a</sup> Mean ± SE (number of paired preparations). The theoretical flux-ratios were calculated from (Ussing, 1949),  $J^{in}/J^{out} = [Cl]_o/[Cl]_i \exp(-FV/RT)$ .

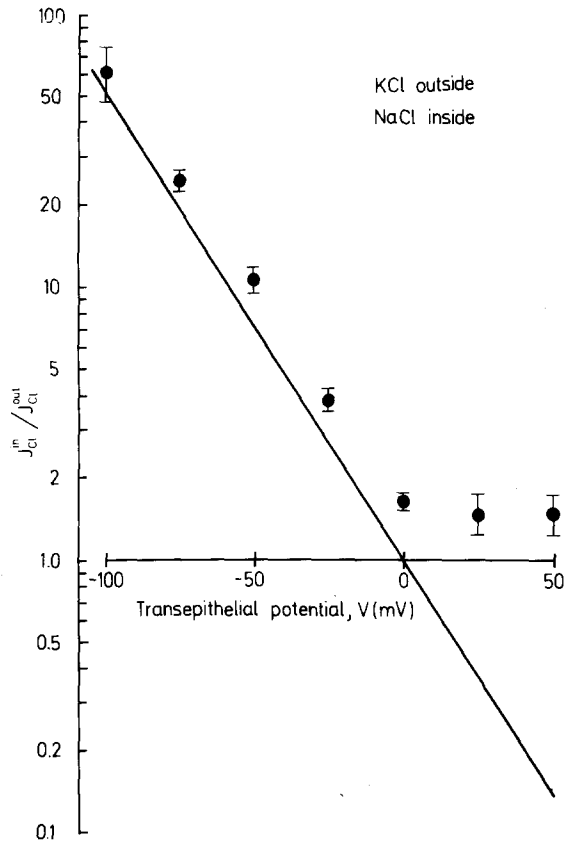


**Fig. 3.** (A) Steady-state current-voltage relationships of toad skin exposed to outside KCl-Ringer's and inside NaCl-Ringer's. The Cl<sup>-</sup> currents were estimated from measurements of unidirectional <sup>36</sup>Cl<sup>-</sup> fluxes. (B) Relationship between estimated Cl<sup>-</sup> currents and clamping currents of toad skin in the negative regions of the current-voltage relationship. The equation of the regression-line is  $I_t = 1.05 I_{Cl} - 2.19 \mu A/cm^2$  ( $n = 28$ )

amounted to  $14.2 \pm 4.7 \mu A/cm^2$  (initial period) and  $30.1 \pm 8.7 \mu A/cm^2$  (final period). It is apparent, therefore, that the cation conductance at  $V = 50$  mV became significantly larger towards the end of these experiments characterized by long-duration voltage clamping at positive potentials.

#### POTENTIAL DEPENDENCE OF THE RATIO OF UNIDIRECTIONAL Cl<sup>-</sup> FLUXES

The asymmetry of the potential dependence of the Cl<sup>-</sup> fluxes was further analyzed from the relation between their ratio and potential (*see* Fig. 4). For  $V$



**Fig. 4.** Dependence of the ratio of unidirectional fluxes on transepithelial potential. The line is drawn according to the theoretical relation for independent fluxes (Ussing, 1949)

$> 0$  mV, the influx as well as the efflux were largely unaffected by  $V$  (Table 1), and the ratios were closer to unity than to the theoretical values for electrodiffusive ion flows. A similar result was obtained with skins exposed to NaCl-Ringer's on both sides (Larsen & Rasmussen, 1982; Dürr & Larsen, 1986) and it strongly indicates that significant components are carried by a 1 : 1 exchange diffusion pathway. In similar agreement with the above studies, the present material reveals an active flux component for  $V = 0$  mV, and an electrodiffusive behavior of the fluxes for  $V < 0$  mV.

#### INFLUENCE OF EXTERNAL IONS ON THE TIME COURSE OF VOLTAGE-CLAMP CURRENTS

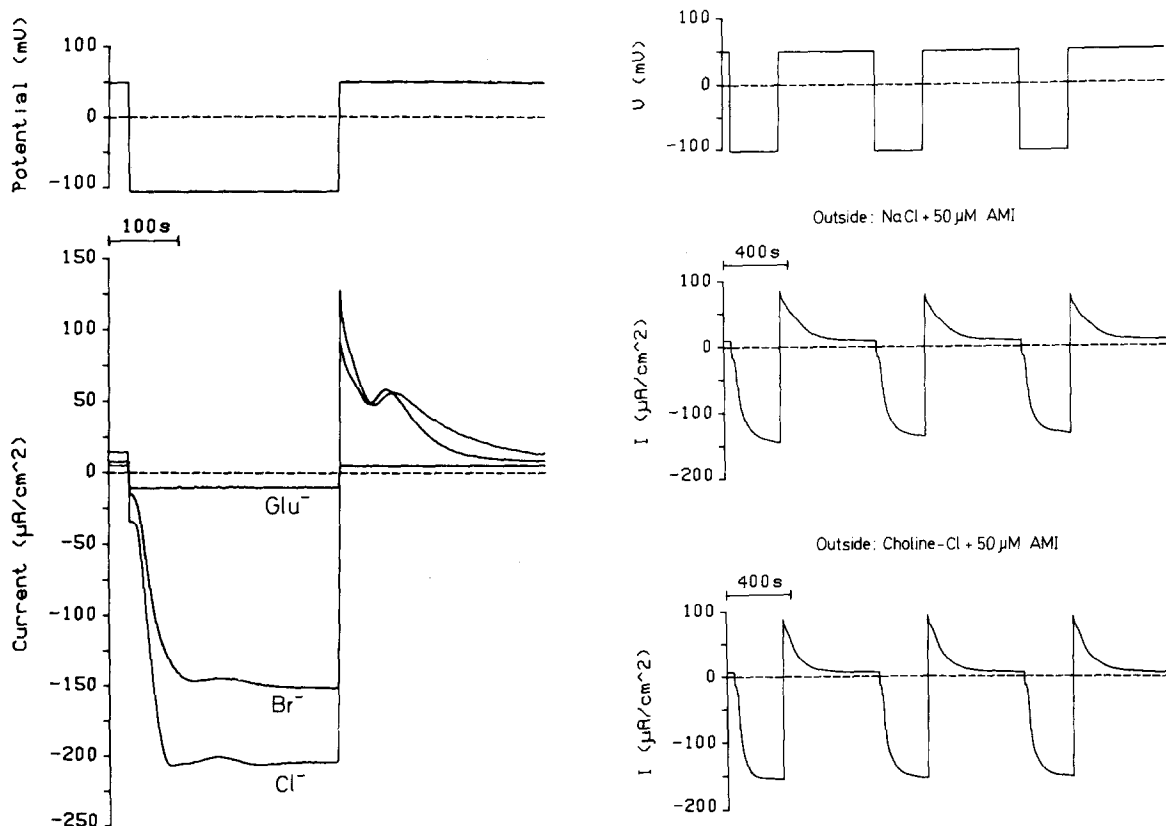
The results above show that the transepithelial  $\text{Cl}^-$  conductive pathway is turned off in skins clamped at  $0 < V < 50$  mV and is activated in the region of

physiological potentials. The time course of the transition from deactivated to the activated state was followed by monitoring the change in clamping current in response to a fast shift of  $V$  from 50 to  $-100$  mV. Figure 5, left panel, shows that these currents are dependent on the major anions in the outer bathing solution. In the presence of chloride or bromide, but not gluconate, the current increased slowly to a new steady state, revealing the slow activation of the anion conductance. It is also seen that the process of activation was fully reversible. Figure 5, right panel, shows that the time course of the voltage-clamp currents and their steady-state values were independent of the major cations in the outer bathing solution. Furthermore, as the peak value of the inward current recorded upon return of  $V$  to 50 mV was independent of whether  $\text{Na}^+$  or choline was present in the outer bath, it is indicated that cations do not pass the voltage-activated pathway.

The above results provide the evidence that the transient currents are carried by  $\text{Cl}^-$  ions across the external border of the epithelium and that this pathway also is permeable for  $\text{Br}^-$ , but not for gluconate. [For a more detailed analysis of the anion selectivity of the  $\text{Cl}^-$  pathway, see Harck and Larsen (1986)].

#### INTRACELLULAR POTENTIAL AND CHLORIDE ACTIVITY IN SHORT-CIRCUITED EPITHELIA

Isolated epithelia from toads adapted to distilled water were impaled from the outside under short-circuit conditions. Figure 6 depicts two impalements of principal cells of a preparation exhibiting a relatively high short-circuit current ( $40 \mu\text{A}/\text{cm}^2$ ). During the first impalement, the recorded intracellular potential was instantaneously  $-50$  mV, but declined to  $-46$  mV within about 100 sec. Within the first 15 to 20 sec of the impalement,  $a_{\text{Cl}^-}^i$  approached 23 mM. During the subsequent impalement, the potential initially reached a value of  $-53$  mV and stayed constant for about 100 sec. In this case the intracellular  $\text{Cl}^-$  activity was 21 mM, i.e. close to the value of the first impalement. With the microelectrode tip in an intracellular position, a brief transepithelial pulse of  $-100$  mV was applied at approximately  $t = 350$  sec giving rise to a  $100\text{-}\mu\text{A}/\text{cm}^2$  deflection of the clamping current and a 73-mV deflection of the reference electrode signal. From the latter the fractional apical membrane resistance can be calculated:  $fR_a = R_a/(R_a + R_b) = \Delta V_a/\Delta V = 0.73$ . The  $a_{\text{Cl}^-}^i$ -trace is seen to show capacitative transients



**Fig. 5.** Left panel: Voltage-clamp currents of toad skin with NaCl-Ringer's inside and KCl Ringer's, KBr-Ringer's or K-gluconate Ringer's outside with the major anions indicated on the graphs. Voltage-clamp program indicated on top. Right panel: As in left panel but with varying cation-composition of the outer bath. The voltage-clamp currents indicate that the time course for the development of the activated Cl<sup>-</sup> conductance is independent of the external cations, and that the activation mechanism is not exhausted by repeated activations

in both directions.<sup>2</sup> The intracellular localization of the electrode tip was confirmed by application of 10<sup>-6</sup> M amiloride to the outer bathing solution leading to a hyperpolarization of V<sub>a</sub> by 10 to 25 mV as depicted in Fig. 7. Amiloride treatment led to no change in a<sub>Cl</sub><sup>i</sup>. Thus, in four preparations (I<sub>sc</sub> = 19.8 ± 1.8 μA/cm<sup>2</sup>) a<sub>Cl</sub><sup>i</sup> was 15.4 ± 3.2 mM and 15.1 ± 2.9 mM before and 25 min after addition of amiloride, respectively.

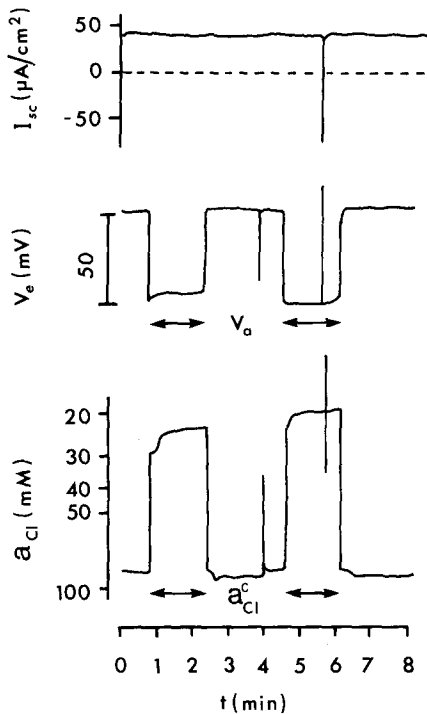
Table 2 collects the results of 24 impalements from six preparations. It is seen that the values scatter considerably between the preparations but little

**Table 2.** Short-circuit current, intracellular potential and chloride activity of principal cells from animals adapted to distilled water

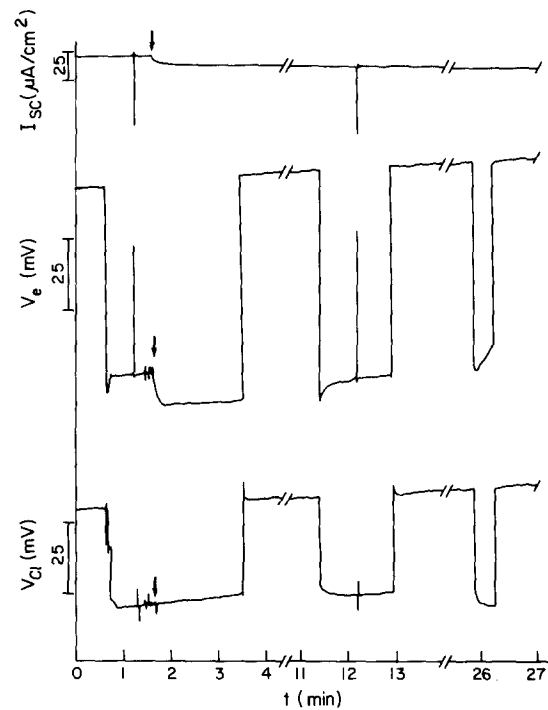
Preparation	I <sub>sc</sub> (μA/cm <sup>2</sup> )	V <sub>a</sub> (mV)	a <sub>Cl</sub> <sup>i</sup> (mM)	n
1	20.0 ± 0.0	-59.0 ± 5.7	16.0 ± 1.9	2
2	24.8 ± 4.4	-54.2 ± 6.4	14.3 ± 1.8	5
3	41.7 ± 2.6	-49.0 ± 3.9	23.4 ± 3.2	6
4	25.8 ± 0.5	-79.5 ± 6.4	17.2 ± 3.9	4
5	17.8 ± 5.6	-95.3 ± 2.1	14.7 ± 2.5	4
6	20.0 ± 0.0	-82.7 ± 4.6	19.6 ± 0.5	3
Mean ± SD	27.0 ± 9.6	-67.9 ± 18.5	18.0 ± 4.4	24
Mean ± SE	27.0 ± 2.0	-67.9 ± 3.8	18.0 ± 0.9	

<sup>2</sup> The much larger capacitance of the resin-filled Cl<sup>-</sup>-selective barrel results in capacitive current transients following voltage perturbations that are much larger than for the electrolyte-filled reference barrel. Furthermore, as the resistance of the Cl<sup>-</sup>-selective barrel is more than 100 times larger than that of the reference barrel, the time constant is so large that the slowly relaxing capacitive current is monitored even by the slow-reponding pen recorder.

within a single preparation. Preparations exhibiting large short-circuit currents tend to have numerically smaller intracellular potentials and higher intracellular Cl<sup>-</sup> activities. In Fig. 8A is shown the relationship between V<sub>a</sub> and I<sub>sc</sub>. These variables were found



**Fig. 6.** Impalements of two principal cells in the short-circuited epithelium. The three panels depict the short-circuit current, the intracellular potential, and the difference between the  $\text{Cl}^-$ -selective barrel and the reference barrel signals converted to  $\text{Cl}^-$  activity.  $V_e$  denotes the reference electrode signal. At  $t = 350$  sec  $V$  is briefly perturbed by  $-100$  mV. Horizontal arrows indicate periods of intracellular recordings



**Fig. 7.** Effect of amiloride addition (arrows) on short-circuit current, apical membrane potential and intracellular  $\text{Cl}^-$  activity within half an hour.  $V_e$  denotes the reference electrode signal. Amiloride hyperpolarizes the membrane potential, from  $-64$  to  $-75$  mV whereas the  $\text{Cl}^-$  activity remains constant at  $19.5$  mM. Ten min after amiloride addition the membrane potential has relaxed to  $-70$  mV.  $a_{\text{Cl}}^c$  is unchanged. After 25 min  $V_a$  is  $-68$  mV and  $a_{\text{Cl}}^c$  is  $15$  mM

to be positively correlated with a value of  $V_a \approx -100$  mV for  $I_{\text{sc}} = 0 \mu\text{A}/\text{cm}^2$ . A plot of  $a_{\text{Cl}}^c$  against  $I_{\text{sc}}$  (Fig. 8B) revealed a positive correlation between these variables with  $a_{\text{Cl}}^c \approx 9$  mM for  $I_{\text{sc}} = 0 \mu\text{A}/\text{cm}^2$ .

#### MEMBRANE POTENTIALS, $\text{Cl}^-$ ACTIVITY AND FRACTIONAL MEMBRANE RESISTANCE DURING ACTIVATION AND DEACTIVATION OF THE $\text{Cl}^-$ CONDUCTANCE

As for the flux-ratio analysis, this series of experiments was conducted with epithelia from animals adapted to a dry milieu with free access to tap water. The epithelium was exposed to KCl-Ringer's on the outside and impaled at a transepithelial clamping potential of  $40$  mV (mucosa positive) at which the transepithelial  $\text{Cl}^-$  conductance ( $G_{\text{Cl}}$ ) is deactivated (Table 1, Figs. 2–5). As an example, Fig. 9 depicts an acceptable impalement. After the initial potential deflections caused by the penetration of stratum corneum, a stable electrode signal of about  $-61$  mV, and a fractional outer membrane resistance of  $0.71$  were obtained. In contrast to the low

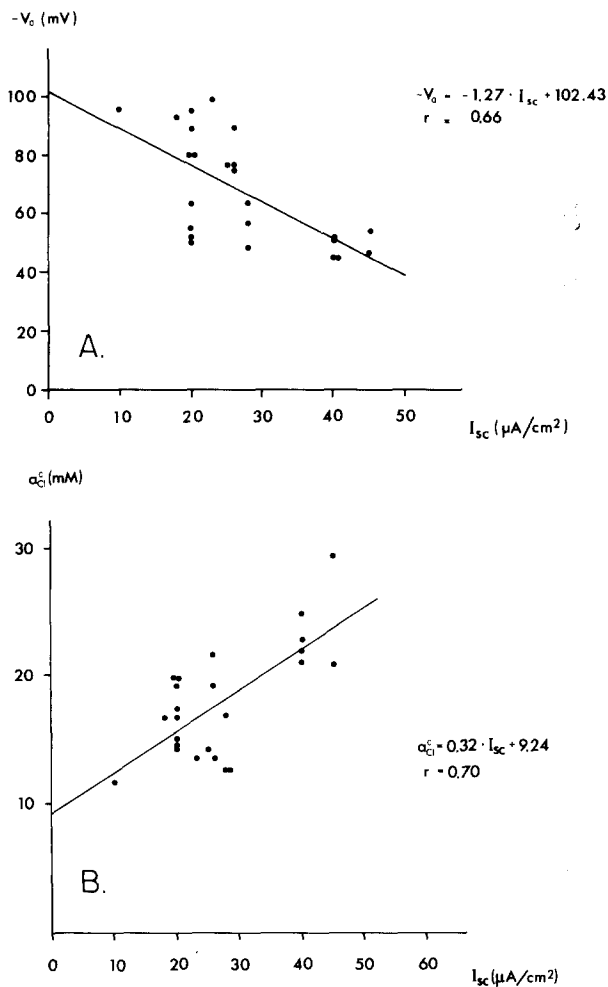
$a_{\text{Cl}}^c$  found in skin from animals adapted to distilled water, epithelia from this group of animals typically showed intracellular  $\text{Cl}^-$  activities of about  $40$  mM. In the example shown,  $a_{\text{Cl}}^c$  was  $42$  mM. At  $t = 120$  sec,  $V$  was stepped to  $-100$  mV resulting in the characteristic sigmoidal increase of the clamping current that is associated with activation of the transepithelial  $\text{Cl}^-$  conductance (see Fig. 5). As the  $\text{Cl}^-$  activities of the outside and inside bathing solution are identical, the voltage-activated  $\text{Cl}^-$  conductance can be estimated by  $G_{\text{Cl}} = \Delta I/V = -88/-100 = 0.88$  mS/cm<sup>2</sup>, i.e. a value close to those obtained for whole skins (Table 1).  $V_a$  changed instantaneously by  $99$  mV, to  $38$  mV, (cell interior positive with respect to the mucosal bath). During the following  $90$  sec,  $V_a$  changed only slightly. Except for a brief capacitative transient, the signal from the  $\text{Cl}^-$ -selective electrode remained unchanged, indicating that  $a_{\text{Cl}}^c$  stayed constant in spite of the large increase of the transepithelial  $\text{Cl}^-$  conductance. Within the following  $90$  sec, no significant change of  $a_{\text{Cl}}^c$  occurred. At  $t = 220$  sec,  $V$  was returned to  $40$  mV resulting in an instantaneous reversal of the clamping current that, in turn, slowly relaxed to its pre-



**Table 3.** Intracellular parameters of toad skin epithelium during activation and deactivation of transepithelial chloride conductance ( $G_{Cl}$ ): KCl-Ringer's outside mean  $\pm$  SE:  $n = 15$

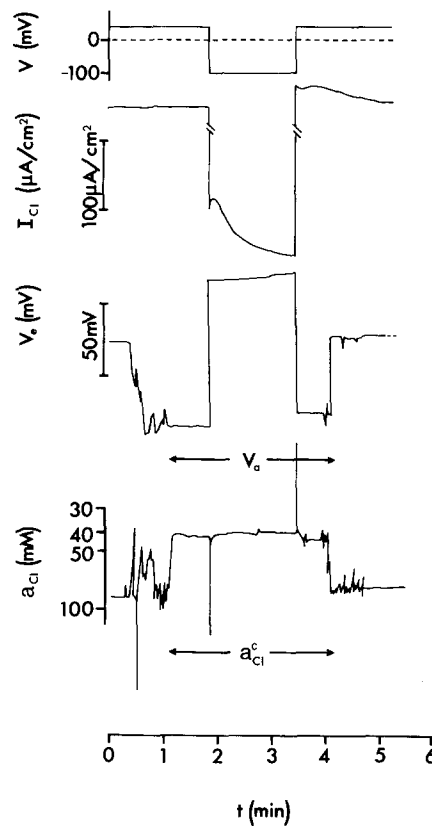
Transepithelial potential, $V$	$V_a$ (mV)	$a_{Cl}^i$ (mM)	$fR_a$	$G_{Cl}$ (mS/cm <sup>2</sup> ) <sup>a</sup>
40 mV, $G_{Cl}$ deactivated	$-70.1 \pm 5.0$	$40.0 \pm 3.8$		
-100 mV before activation of $G_{Cl}$	$31.3 \pm 5.6$	$42.3 \pm 4.3$	$0.69 \pm 0.03$	
-100 mV after activation of $G_{Cl}$	$27.1 \pm 6.4$	$41.4 \pm 4.3$		$1.19 \pm 0.10$
40 mV before deactivation of $G_{Cl}$	$-67.8 \pm 3.9$	$38.9 \pm 4.4$	$0.67 \pm 0.03$	

<sup>a</sup>  $G_{Cl}$  was determined as the difference in the transepithelial conductance measured at -100 and 40 mV, respectively.



**Fig. 8.** (A) Relation between the intracellular potential under short-circuit conditions and the short-circuit current. The regression line is given by  $-V_a = -1.27 \times I_{sc} + 102.43$  ( $r = 0.66$ ). (B) Relationship between intracellular Cl<sup>-</sup> activity and short-circuit current. The regression line is given by  $a_{Cl}^i = 0.32 \times I_{sc} + 9.24$  ( $r = 0.70$ )

pulse steady-state value, illustrating that the conductance activation was fully reversible. The reference electrode potential instantaneously re-



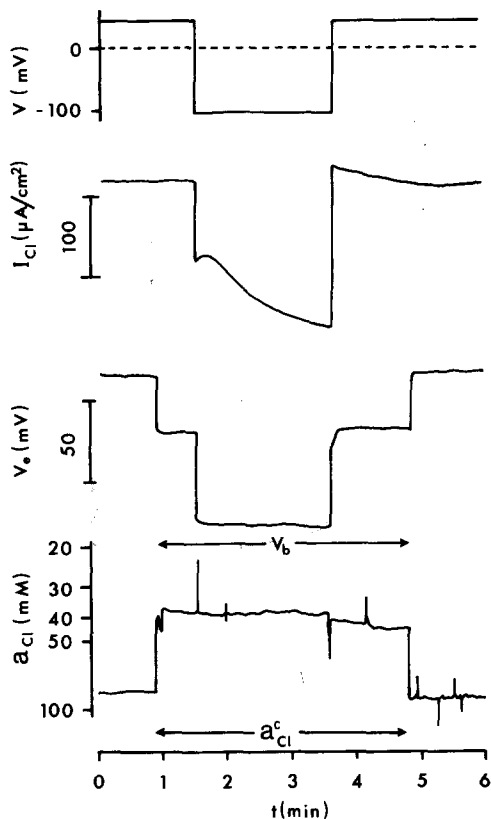
**Fig. 9.** Simultaneous recordings of the voltage-clamped transepithelial potential, the short-circuit current, the apical membrane potential ( $V_a$  denotes reference electrode signal) and the intracellular Cl<sup>-</sup> activity during activation and deactivation of the transepithelial Cl<sup>-</sup> conductance by shifting  $V$  from 40 to -100 mV, and back

turned to a value slightly less than that prior to the  $G_{Cl}$  activation, and remained constant. The Cl<sup>-</sup> electrode potential again exhibited a capacitive deflection, but remained thereafter constant at a slightly depolarized value. After 30 sec, the electrode was withdrawn and both electrode potentials returned to values close to their original baseline values. In Table 3 is shown the mean values of  $V_a$ ,  $a_{Cl}^i$ ,  $fR_a$  and the increase of  $G_{Cl}$  from 15 imple-

**Table 4.** Basolateral membrane potential, fractional membrane resistance and intracellular Cl<sup>-</sup> activity of the principal cells at deactivated and activated G<sub>Cl</sub>; impalements from the inside

$V_b(40 \text{ mV})$ (mV)	$V_b(-100 \text{ mV})$ (mV)	$\Delta V_b$ (mV)	$fR_b$	$fR_a$	$a_{\text{Cl}}^c$ (mM)
-34	-91	-57	0.41	0.59	36
-45	-90	-45	0.32	0.68	28
-40	-75	-35	0.26	0.74	33
-56	-91	-35	0.26	0.74	32
-62	-99	-37	0.26	0.74	26
-45	-90	-45	0.32	0.68	32
-55	-82	-27	0.19	0.81	32
-18	-45	-27	0.19	0.81	32
-26	-44	-18	0.15	0.85	30
-21	-45	-24	0.17	0.83	31
$-40.2 \pm 4.8^a$	$-75.2 \pm 7.0$	$-35.0 \pm 3.7$	$0.25 \pm 0.03$	$0.75 \pm 0.03$	$31.2 \pm 0.9$

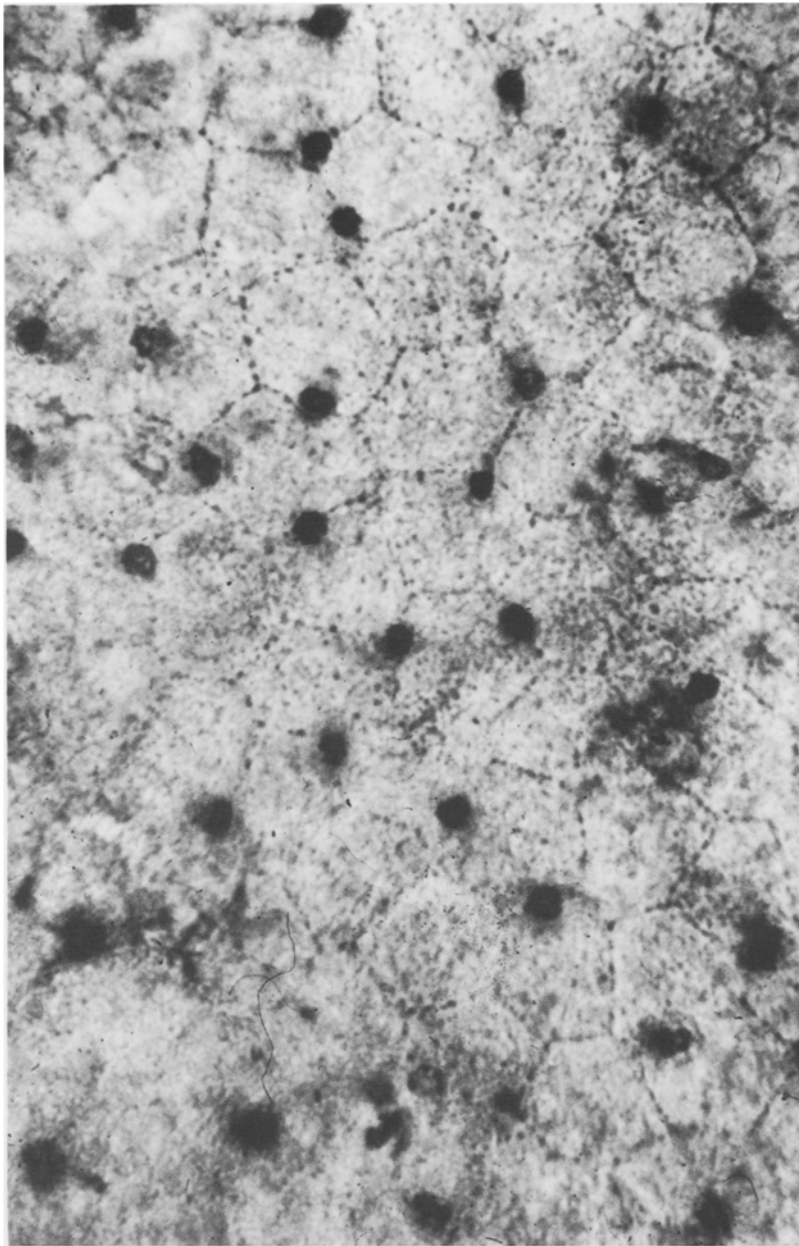
<sup>a</sup> Mean  $\pm$  SE;  $n = 10$ .

**Fig. 10.** Impalement of a stratum germinativum cell from the inside. Same protocol as in Fig. 9

ments. It can be seen that the imposed change of the transepithelial potential from 40 to  $-100 \text{ mV}$  instantaneously shifted  $V_a$  by  $101.4 \text{ mV}$  from  $-70.1 \pm 5.0 \text{ mV}$  to  $31.3 \pm 5.6 \text{ mV}$ . During the next 2 to 5 min, while  $G_{\text{Cl}}$  became nearly maximally activated,  $V_a$  did not change significantly ( $P > 0.1$ ). Likewise,  $a_{\text{Cl}}^c$  stayed constant ( $P > 0.1$ ) irrespective of whether  $G_{\text{Cl}}$  was deactivated ( $40 \text{ mV}$ ) or nearly maximally

activated (new steady state at  $-100 \text{ mV}$ ). Also  $fR_a$  was independent of the transepithelial conductance ( $0.67$  compared to  $0.69$ ). Returning  $V$  to  $40 \text{ mV}$  resulted in an instantaneous shift in  $V_a$  by  $94.9$  to  $-67.8 \text{ mV}$  which is not significantly different from  $V_a$  recorded before stepping the transepithelial potential to  $-100 \text{ mV}$ .

As the cells are impaled from the outside bath, the microelectrode is advanced through the cornified layer of cells. This leads to a significant distortion of the epithelium that might have influenced the conductive properties of the cell membranes. In another series of experiments, therefore, the epithelium was impaled from the serosal side. Figure 10 depicts an impalement fulfilling our criteria. At  $t = 60 \text{ sec}$  the cell was impaled and the basolateral membrane potential ( $V_b$ ) was found to be  $-34 \text{ mV}$ . The intracellular Cl<sup>-</sup> activity was  $38 \text{ mM}$ , i.e. close to the value determined from impalements from the outside. After approximately  $40 \text{ sec}$  the clamping potential was shifted from  $40$  to  $-100 \text{ mV}$  causing a hyperpolarization of  $V_b$  by  $-57$  to  $-91 \text{ mV}$ . The difference signal of the two barrels varied but little, indicating that  $a_{\text{Cl}}^c$  remained almost constant during the transition of the epithelium to a new steady state. After about  $120 \text{ sec}$ ,  $G_{\text{Cl}}$  was nearly maximally activated and  $V$  was stepped back to  $40 \text{ mV}$ , which led to a return of  $V_b$  to  $-34 \text{ mV}$ . During the following minute,  $V_b$  remained constant whereas  $a_{\text{Cl}}^c$  increased somewhat. However, following electrode withdrawal it was seen that also the baseline for the Cl<sup>-</sup>-selective electrode signal had changed a comparable amount, indicating that the intracellular Cl<sup>-</sup> activity, also in this case, changed but little during the sequence of Cl<sup>-</sup> conductance activation/deactivation. Qualitatively, the observed behavior of  $V_b$  and  $a_{\text{Cl}}^c$  is in agreement with that observed during impalements from the outside. Table 4 summarizes the results of 10 impalements. It is seen that the



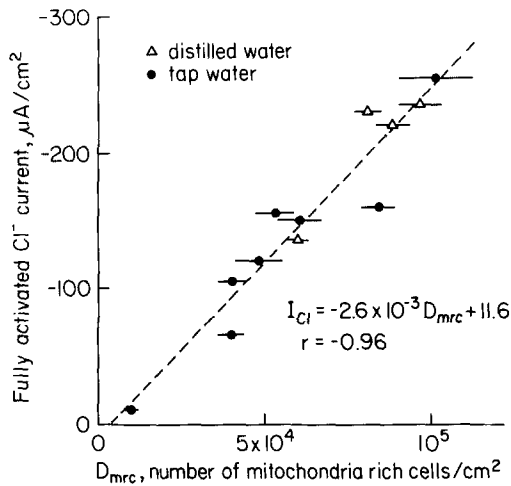
**Fig. 11.**  $\text{Ag}^+$ -stained toad skin epithelium. Mitochondria-rich cells are clearly visible. Note the small surface area of the m.r. cells compared to the granulosum cells

observed potential profiles determined by impalement from the outside and inside, respectively, are quantitatively in agreement. However,  $a_{\text{Cl}}^{\text{c}}$  was found to be somewhat lower, 31.2 mM, in the germinativum cells.

#### $\text{Ag}^+$ STAINING OF THE MITOCHONDRIA-RICH CELLS

Due to their small size and scattered distribution beneath the cornified cells it was not possible for us to impale the m.r. cells. Additionally, they were pushed out of focus as the micropipettes were ad-

vanced through the stratum corneum. Therefore we chose another experimental approach for investigating their possible role in transepithelial  $\text{Cl}^-$  transport. These cells have for long been known to be selectively stained by silver ions (Rudneff, 1865).  $\text{Ag}^+$  is also known to stain selectively the apical crypt of the fish gill chloride cells (Philpott, 1965), and the chloride cells of the fish opercular membrane (our own *unpublished observations*). Recently, the latter cell type was shown to secrete  $\text{Cl}^-$  ions (Scheffey et al., 1983). The  $\text{Ag}^+$  staining mechanism is believed to reflect the precipitation of  $\text{AgCl}$  directly outside the membrane areas having a significant  $\text{Cl}^-$  permeability. Besides the m.r. cells,



**Fig. 12.** Relationship between the current through the fully activated  $\text{Cl}^-$  conductance ( $V = -100$  mV) and the density of m.r. cells. Each point indicates the mean  $D_{\text{MRC}}$  observed in animals adapted to tap water (●) or distilled water (△). The regression line is given by  $I_{\text{Cl}} = -2.6 \times 10^{-3} \times D_{\text{MRC}} + 11.6$  ( $r = -0.96$ ).

the tight junction areas were also found to be slightly stained (Fig. 11). Probably, this reflects the nonselective increase of the paracellular permeability due to  $\text{Ag}^+$  exposure reported from frog skin (Curran, 1972) and corneal epithelium (Klyce & Marshall, 1982). In six experiments in which the skins prior to  $\text{Ag}^+$  exposure had been bathed on both sides with  $\text{Cl}^-$ -free Ringer's for 2 hr, we found no silver staining of the m.r. cells. The staining method itself, thereby, indicates that the apical membrane of the m.r. cells is permeable to  $\text{Cl}^-$  ions, whereas the apical membrane of the outermost principal cells is not.

In skins from 12 animals adapted to either tap water or distilled water we determined the density of m.r. cells ( $D_{\text{MRC}}$ ) and the  $\text{Cl}^-$  current flowing through the fully activated chloride conductance at  $-100$  mV. A linear correlation between these parameters (Fig. 12), characterized by a correlation coefficient of  $-0.96$  and a slope of  $-2.5$  nA per m.r. cell, was found. Both  $D_{\text{MRC}}$  and the  $\text{Cl}^-$  current of skins adapted to distilled water was generally higher than those from skins adapted to tap water.

## Discussion

### COMPONENTS OF THE TRANSEPITHELIAL $\text{Cl}^-$ FLUXES

The potential dependence of the  $\text{Cl}^-$  current (Fig. 3) and of the  $\text{Cl}^-$  flux ratio (Fig. 4) reveal different modes of  $\text{Cl}^-$  transport through the toad skin bathed

with KCl-Ringer's on the outside. Thus, at potentials above 0 mV the net flux of  $\text{Cl}^-$  was not significantly different from zero in spite of a measurable tissue conductance reflected in the  $I$ - $V$  relation shown in Fig. 3A. These steady-state currents, observed under conditions of no  $\text{Cl}^-$  net flux are most likely carried by  $\text{K}^+$  through the principal cells (Zeiske & Van Driessche, 1979; Nagel & Hirschmann, 1980; Van Driessche & Zeiske, 1980), and the  $\text{Cl}^-$  fluxes are most likely carried by a  $\text{Cl}^-/\text{Cl}^-$  exchange transport system.

The active  $\text{Cl}^-$  component, revealed at  $V = 0$  mV, is of a small magnitude,  $I_{\text{Cl}} = -1.8 \pm 0.31 \mu\text{A}/\text{cm}^2$ , but it is equal to the value of the short-circuited frog skin bathed with choline-Ringer's outside,  $I_{\text{Cl}} = -2.6 \pm 1.2 \mu\text{A}/\text{cm}^2$  (Drewnowska & Biber, 1985), and short-circuited toad skin exposed to NaCl-Ringer's with  $50 \mu\text{M}$  amiloride on the outside,  $I_{\text{Cl}} = -1.6 \pm 0.3 \mu\text{A}/\text{cm}^2$  (Dürr & Larsen, 1986). All of these values are smaller than the active  $\text{Cl}^-$  currents in short-circuited skins exposed to bilateral NaCl-Ringer's,  $I_{\text{Cl}} = -5.2 \pm 1.5 \mu\text{A}/\text{cm}^2$  (toad skin, Bruus et al., 1976), and  $I_{\text{Cl}} = -12.3 \pm 3.1 \mu\text{A}/\text{cm}^2$  (frog skin, Drewnowska & Biber, 1985). The above studies provide additional examples that active  $\text{Cl}^-$  transport can occur in the isolated short-circuited amphibian skin, as first demonstrated by Zadunaisky and co-workers (Zadunaisky et al., 1963). A possible dependence of the active  $\text{Cl}^-$  flux on active transport of  $\text{Na}^+$  was discussed by Harvey and Kernan (1984), Drewnowska and Biber (1985), and Biber et al. (1985) and they suggested that an electroneutral transport system is localized to the apical membrane of the outermost principal cell layer (for further discussion, see below).

In the physiological range of potentials ( $V < 0$  mV), the activated  $\text{Cl}^-$  conductance directed the total current across the epithelium (Fig. 3). The flux-ratio analysis indicated that these large currents are predominantly passive (Fig. 4), in agreement with the result of previous studies with skins exposed to bilateral NaCl-Ringer's (Larsen & Rasmussen, 1982; Kristensen, 1983; Dürr & Larsen, 1986) or to 1/10 NaCl-Ringer's on the outside (Koefoed-Johnsen et al., 1952a). This conclusion is also in agreement with the low temperature coefficient ( $Q_{10}$ ) of these currents; in nine preparations,  $Q_{10}$  ranged from 1.1 to 1.5 (Willumsen & Larsen, 1982).

### APICAL MEMBRANE POTENTIAL IN STEADY STATE

Intracellular potentials of amphibian skin have been reported during the last three decades. As discussed by Nagel (1979) studies until 1975 often reported small intracellular potentials ( $-10$  mV  $< V_a < -40$  mV) under short-circuit conditions, and trans-

epithelial potential profiles of the staircase type under open-circuit conditions. Selection of microelectrodes with small tip-diameter (for discussion, see Nelson et al., 1978) and establishment of more strict criteria for acceptance of measurements (Nagel, 1976; Helman & Fisher, 1977) has led to considerably increased values of reported intracellular potentials. Thus, Nagel (1975, 1977) and Helman and Fisher (1977) concordantly reported  $V_a$  values in the order of  $-100$  mV under short-circuit conditions and a well-type potential profile under open-circuit conditions. Since then it has been generally accepted that  $V_a$  on the average is somewhere between  $-60$  and  $-80$  mV (Nagel, 1976; Nagel et al., 1981; Giraldez & Ferreira, 1984). However, typically a broad interval of  $V_a$  values is reported in each study, (Nagel, 1976; Garcia-Diaz et al., 1985). Nagel (1976), for instance, reports 67 measurements in the interval  $-113$  mV  $< V_a < -32$  mV with a mean value of  $-73$  mV in frog skin exposed to NaCl-Ringer's on both sides. In the present study, we found  $V_a$  values in the interval  $-98$  mV  $< V_a < -45$  mV and a mean of  $-67.9$  mV. Among epithelia of different animals the mean  $V_a$  varied from  $-95.3$  to  $-49.0$  mV (Table 2). Only little variation of membrane potentials was seen among cells of the individual preparations.

The variation of  $V_a$  was found to be correlated with the short-circuit current as was also found by Nagel (1976). Animals having large  $I_{sc}$  exhibited small intracellular potentials and vice versa (Fig. 8A). This relationship most likely reflects that variation in  $I_{sc}$  is caused by a variation of the apical membrane Na<sup>+</sup> permeability. Accordingly, the intercept of  $-100$  mV (Fig. 8A) is a measure of the K<sup>+</sup> equilibrium potential giving an intracellular K<sup>+</sup> concentration  $K_c = K_i \cdot \exp(-FE_K/RT) \approx 2.4 \cdot \exp(-96,500 \times (-0.1)/(8.31 \times 295)) = 123$  mM, in reasonably good agreement with values reported from electron microprobe studies of toad skin (Rick et al., 1980). In agreement with this notion, as  $P_{Na}^a$  was decreased by adding  $10^{-4}$  M amiloride to the mucosal bath,  $V_a$  hyperpolarized by 10 to 25 mV (Fig. 7) as reported by others (Nagel et al., 1981; Garcia-Diaz et al., 1985).

With KCl-Ringer's on the outside, and  $V$  clamped to 40 mV (mucosa positive) we recorded, on the average, an apical membrane potential of  $-71 \pm 5$  and  $-80 \pm 5$  mV by impalements from the outside and the inside, respectively. This reveals a mean basolateral membrane potential of  $-31$  and  $-40$  mV, respectively, i.e. significantly smaller than the estimated  $V_b$  with NaCl outside. Most likely, these small values of  $V_b$  reflect a reduced inner membrane K<sup>+</sup> permeability, whereby the membrane potential is driven towards the equilibrium potentials of the two other diffusible ions (Na<sup>+</sup> and

Cl<sup>-</sup>). Support for this interpretation comes from a recent study by Davis and Finn (1982) showing that in the toad urinary bladder reduction of the Na<sup>+</sup> conductance (amiloride) of the apical membrane leads to a decrease of the K<sup>+</sup> conductance of the basolateral membrane, whereby the cells become depolarized.

#### INTRACELLULAR Cl<sup>-</sup> ACTIVITY UNDER SHORT-CIRCUIT CONDITIONS

Under short-circuit conditions the mean  $a_{Cl}^c$  was found to be 18 mM in skins from toads adapted to distilled water. This pretreatment is known to stimulate the passive transepithelial Cl<sup>-</sup> conductance (Fig. 12, Katz & Larsen, 1984). The value for  $a_{Cl}^c$ , which is equivalent to an intracellular Cl<sup>-</sup> concentration of 23 mM if the cell Cl<sup>-</sup> activity coefficient equals that in free solution (0.76), is in agreement with those of other microelectrode studies (Nagel et al., 1981; Giraldez & Ferreira, 1984; Harvey & Kernan, 1984), but far below the values measured by other techniques, for instance wash-out experiments (Ferreira & Ferreira, 1981; Stoddard & Helman, 1982) and electron microprobe analyses (Rick et al., 1978, 1980; Dörge et al., 1985), which lead to intracellular concentrations in the order of 40 to 50 mM. Table 5 summarizes  $a_{Cl}^c$  determinations from the literature. The reason for the discrepancy between the two groups of methods is at present unknown. The discrepancy becomes even larger if, as shown by Spring and Kimura (1978) and McCaig and Leader (1984), the Cl<sup>-</sup> activities measured with liquid ion exchanger (Orion) microelectrodes should be corrected for a value of approximately 4 to 6 mM due to interfering cytoplasmic anions (e.g. bicarbonate, acetate, propionate, and isethionate). No major Cl<sup>-</sup> pool seems to be physically or chemically compartmentalized within the cells as a total exchangeable Cl<sup>-</sup> pool of 40 to 50 mM was shown to be osmotically active (MacRobbie & Ussing, 1961; Ussing, 1985). However, all estimates of  $a_{Cl}^c$  yield values far above the equilibrium activity. Employing the measured  $V_a$  value of  $-68$  mV, the theoretical thermodynamic intracellular equilibrium activity is calculated to be approximately 5.5 mM. Based on this observation, together with the demonstration of a low apical membrane Cl<sup>-</sup> permeability (Ferreira & Ferreira, 1981) and the responses of cell volume (Ussing, 1982) and  $a_{Cl}^c$  (Dörge et al., 1985) to furosemide or bumetanide in the inner bath, the existence of a basolateral NaCl cotransport system in the principal cells was suggested. The cotransport system which is supposedly equivalent to the type described from other cell types, for instance gall-bladder (Frizzell et al., 1979) and Ehrlich ascites tu-

**Table 5.** Intracellular chloride activities and concentrations reported from amphibian skin

Reference	Species	$a_{Cl}$ (mM)	$c_{Cl}$ (mM)	$n$	Conditions <sup>a</sup>	Method
MacRobbie & Ussing (1961)	<i>R. temporaria</i>		49 ± 2	6	o.c.	Osmotic method
Ussing (1985)	<i>R. temporaria</i>		41		o.c.	
Nagel et al. (1981)	<i>R. pipiens</i>	18 ± 3		5	s.c.	Ionselective
Giraldez & Ferreira (1984)	<i>R. ridibunda</i>	21.9 ± 1.5		5	s.c.	Ionselective
Harvey & Kernan (1984)	<i>R. temporaria</i>	20.3 ± 1.6		60	o.c.	microelectrodes
Biber et al. (1985)	<i>R. pipiens</i>	15.5 ± 0.5		102	s.c.	
Present study	<i>B. bufo</i>	18.0 ± 4.4		24	s.c.	
Present study	<i>B. bufo</i>	40.0 ± 3.8		15	V = 40 mV	
Present study	<i>B. bufo</i>	31.2 ± 0.9 <sup>b</sup>		10	V = 40 mV	
Zylber et al. (1973)	<i>L. ocellatus</i>		57.2 ± 5.3	11	i.c.	Chemical analysis
Ferreria & Ferreira (1981)	<i>R. ridibunda</i>		47.0 ± 2.9	10	s.c.	Washout experiments
			59.8 ± 3.8	8		
Stoddard & Helman (1982)	<i>R. pipiens</i>		42		s.c.	
Rick et al. (1978)	<i>R. temporaria</i>		48 ± 7 <sup>c</sup>	19	s.c.	Electron microprobe analysis <sup>f</sup>
	<i>R. esculenta</i>					
Rick et al. (1980)	<i>B. viridis</i>		52 ± 6 <sup>d</sup>	27	s.c.	
Dörge et al. (1985)	<i>R. temporaria</i>		51 ± 3 <sup>e</sup>	>20		

<sup>a</sup> o.c. = open circuit, s.c. = short circuit, i.c. = isolated cells.

<sup>b</sup> Germinativum cells impaled from the basolateral side.

<sup>c</sup> 36.5 ± 5.0 mmol/kg wet mass.

<sup>d</sup> 39.9 ± 4.9 mmol/kg wet mass.

<sup>e</sup> 39.1 ± 2.7 mmol/kg wet mass (mean ± 2 SEM).

<sup>f</sup> The electron microprobe values are multiplied by 1.3 (conf. references) in order to express the concentration as mmol/liter cell water volume.

mor cells (Hoffmann et al., 1983), transports electrically silent Na<sup>+</sup>, K<sup>+</sup> and 2Cl<sup>-</sup> (Geck et al., 1980) from the serosal compartment into the principal cell compartment driven by the Na<sup>+</sup> gradient across the basolateral membrane (Ussing, 1985).

The observed correlation at steady state, between  $a_{Cl}^i$  and  $I_{sc}$  ( $r = 0.70$ ) (Fig. 3B) is in accordance with the findings of Harvey and Kernan (1984). The interdependence of the intracellular Cl<sup>-</sup> activity and the short-circuit current is not intuitively comprehended from the above theory, because the intracellular potential ( $V_o$ ) and Na<sup>+</sup> activity ( $a_{Na}^i$ ) may change with the apical membrane Na<sup>+</sup> permeability (the short-circuit current). We expect, therefore, that the passive (depending on  $V_o$ ) as well as the active (depending on  $a_{Na}^i$ ) Cl<sup>-</sup> flux components across the basolateral membrane have new values at different steady states.

#### MEMBRANE POTENTIAL AND Cl<sup>-</sup> ACTIVITY DO NOT REFLECT THE DYNAMICS OF $G_{Cl}$

In the short-circuited frog skin amiloride inhibits the active Na<sup>+</sup> transport, and reduces the unidirectional Cl<sup>-</sup> fluxes, as well (Candia, 1978; Kristensen, 1978). A similar reduction of the Cl<sup>-</sup> fluxes

was observed in response to substitution of external Na<sup>+</sup> by a nonpermeating cation (Macey & Meyers, 1963; Kristensen, 1978; Ques-von Petery et al., 1978). These observations indicate that the transepithelial Cl<sup>-</sup> fluxes take a transcellular route and that the cells involved take part in the active Na<sup>+</sup> transport.

The principal cells, which constitute the major cell population of the epithelium, are responsible for the active amiloride-inhibitable Na<sup>+</sup> transport and, therefore, meet a necessary requirement of being the Cl<sup>-</sup> transporting cell type mentioned above. However, our experiments show that the fractional apical membrane resistance of these cells which is of the same size as reported by others (e.g., Nagel et al., 1981) does not change significantly within a period of 2 to 5 min following a 140-mV shift in the clamped transepithelial potential, despite the fact that  $G_{Cl}$  in the same period of time increases by 1.19 mS/cm<sup>2</sup> (from the deactivated to the fully activated state). If, for instance, a major voltage-dependent Cl<sup>-</sup> conductance residing in the apical membrane of the principal cells was responsible for the observed increase in the transepithelial Cl<sup>-</sup> conductance this increase would be paralleled by a significant reduction of  $fR_a$ .

**Table 6.** Cellular chloride activity, membrane potentials, electrochemical Cl<sup>-</sup> potential differences and driving forces across the membranes of the principal cells during activation of the transepithelial Cl<sup>-</sup> conductance in toad skin

Transepithelial potential, $V$ (mV)	$a_{\text{Cl}}^{\text{e}*}$ (mM)	$V_a = \psi_c - \psi_o^*$ (mV)	$V_b = \psi_c - \psi_i$ (mV)	$\Delta\bar{\mu}_{\text{Cl}}^{\text{a}\dagger}$	$\Delta\bar{\mu}_{\text{Cl}}^{\text{b}}$ (Joule/mole)	$\Delta\bar{\mu}_{\text{Cl}}^{\text{a}}/F$	$\Delta\bar{\mu}_{\text{Cl}}^{\text{b}}/F$ (mv)
+40	40 ± 4	-71 ± 3	-31 ± 3	5033	-1173	-52	12
-100 before activation of $G_{\text{Cl}}$	42 ± 4	31 ± 5	-67 ± 5	-4884	-4766	51	49
-100 after activation of $G_{\text{Cl}}$	41 ± 4	29 ± 6	-71 ± 6	-4557	-5093	47	53

\* Mean ± SE;  $n = 15$ .†  $\Delta\bar{\mu}_{\text{Cl}}^{\text{a}} = \bar{\mu}_{\text{Cl}}^{\text{c}} - \bar{\mu}_{\text{Cl}}^{\text{o}} = RT \ln(a_{\text{Cl}}^{\text{c}}/a_{\text{Cl}}^{\text{o}}) - F(\psi_c - \psi_o)$ ;  $\Delta\bar{\mu}_{\text{Cl}}^{\text{b}} = \bar{\mu}_{\text{Cl}}^{\text{c}} - \bar{\mu}_{\text{Cl}}^{\text{i}} = RT \ln(a_{\text{Cl}}^{\text{c}}/a_{\text{Cl}}^{\text{i}}) - F(\psi_c - \psi_i)$ ;  $R = 8.31 \text{ J} \cdot \text{mol}^{-1} \cdot \text{K}^{-1}$ ;  $T = 295 \text{ K}$ ;  $F = 96,500 \text{ Coul} \cdot \text{eqv}^{-1}$ ;  $a_{\text{Cl}}^{\text{i}} = a_{\text{Cl}}^{\text{o}} = 0.74 \times 113 \text{ mM} = 84 \text{ mM}$  (Ringer's solution).

Furthermore, the finding of an  $a_{\text{Cl}}^{\text{e}}$  far above that of passive distribution suggests active accumulation of Cl<sup>-</sup> ions in the principal cell compartment with small dissipative Cl<sup>-</sup> permeabilities of the cell membranes. We estimated the passive driving force for Cl<sup>-</sup> ion flow across the apical and the basolateral membrane at  $V = 40 \text{ mV}$  and  $V = -100 \text{ mV}$ , respectively. The driving force was calculated by  $-\Delta\bar{\mu}/F$ , where  $\Delta\bar{\mu}$  is the estimated difference in electrochemical potential for Cl<sup>-</sup> across the membrane and  $F$  is the Faraday. It is seen (Table 6) that shifting  $V$  from 40 to  $-100 \text{ mV}$  resulted in a change of the driving force across the apical membrane from  $-52 \text{ mV}$  (outward direction) to  $51 \text{ mV}$  (inward direction). The driving force across the basolateral membrane changed from 12 to  $49 \text{ mV}$  (both being directed from cell to serosal bath). Despite these considerable changes of the driving force for Cl<sup>-</sup> flow no change in  $a_{\text{Cl}}^{\text{e}}$  was seen during the transition to a new steady state, suggesting low Cl<sup>-</sup> permeabilities of both membranes. In agreement with the observations of Nagel et al. (1981) and Dörge et al. (1985) we find that exposure of the short-circuited skin to amiloride does not change  $a_{\text{Cl}}^{\text{e}}$  significantly within half an hour despite the subsequent hyperpolarization of  $V_a$  that causes an increased driving force for Cl<sup>-</sup> flow out of the cells. A small apical membrane Cl<sup>-</sup> permeability was also suggested by Biber et al., 1985, who found that the intracellular Cl<sup>-</sup> activity of the short-circuited frog skin did not drop in the absence of mucosal Cl<sup>-</sup> ions. The relatively large  $P_{\text{Cl}}$  of the basolateral membrane reported by Ferreira and Ferreira (1981) and Giraldez and Ferreira (1984) from washout experiments using Cl<sup>-</sup>-free inner solutions might reflect Cl<sup>-</sup> leaving the cellular compartment by the cotransport system as a consequence of the reversed gradient for Cl<sup>-</sup> across the basolateral membrane. Recently, Stoddard et al. (1985) have reported large, fairly symmetrical and electrically silent Cl<sup>-</sup> fluxes across the basolateral membrane of the frog skin. These fluxes, that were inhibited by furosemide and SITS (4-acetamido-4'-isothiocyano-stilbene-2,2'-disul-

fonic acid) were concluded to result from either a Cl<sup>-</sup>/Cl<sup>-</sup> or a Cl<sup>-</sup>/HCO<sub>3</sub><sup>-</sup> exchange mechanism. The presence of such a Cl<sup>-</sup> transport system would not necessarily lead to changes in  $a_{\text{Cl}}^{\text{e}}$  in response to a change in the potential profile and is therefore not in contradiction with the conclusion of our study. Thus, the lack of change in  $a_{\text{Cl}}^{\text{e}}$  in answer to large perturbations of the electrical gradients across the membranes adds further evidence against the hypothesis of a major electrodiffusive Cl<sup>-</sup> transport pathway being located in the principal cells.

Under certain conditions, for instance when the skin is stimulated by epinephrine (Koefoed-Johnsen et al., 1952a) or isoproterenol (Thompson & Mills, 1983), the skin glands are involved in an outward-directed active Cl<sup>-</sup> transport. However, the voltage-dependent Cl<sup>-</sup> pathway cannot be localized to the cells of the skin glands which are embedded deeply into the subepithelial connective tissue, the corium, as the isolated epithelium retains the Cl<sup>-</sup>-transporting characteristics of the intact skin despite the fact that both the mucous glands and the poison glands are normally left in the corium when the epithelium is isolated by collagenase treatment (Carasso et al., 1971).

#### LOCALIZATION OF THE VOLTAGE-DEPENDENT $G_{\text{Cl}}$

Two lines of experimental evidence lead to the hypothesis that the Cl<sup>-</sup> fluxes pass through the mitochondria-rich cells. Exposure of the apical side to amiloride, or substitution of external Na<sup>+</sup> by a non-permeant cation inhibit the unidirectional Cl<sup>-</sup> fluxes through the short-circuited skin. Theoretical treatments (Candia, 1978; Kristensen, 1982) predict that the intracellular hyperpolarization associated with elimination of the apical membrane Na<sup>+</sup> conductance, result in a significant decrease of unidirectional equilibrium Cl<sup>-</sup> fluxes through the cell. Conversely, activation of the Na<sup>+</sup> conductance of the apical membrane of an epithelial cell that is permeable for Cl<sup>-</sup> ion flow, is predicted to result in increased equilibrium Cl<sup>-</sup> fluxes under short-circuit

**Table 7.** Densities of mitochondria-rich cells ( $D_{MRC}$ ) of amphibian skin epithelia

Reference	$D_{MRC}(\text{cm}^{-2})$	Species
Whitear (1975)	213.600 <sup>a</sup>	<i>R. temporaria</i>
Brown et al. (1981)	37.000–198.000 <sup>b</sup>	<i>R. temporaria</i>
	134.000–232.000 <sup>c</sup>	<i>X. laevis</i>
Eskesen ( <i>unpublished</i> )	2.000–180.000 <sup>d</sup>	<i>R. temporaria</i>
Present study	9.900–100.600 <sup>d</sup>	<i>B. bufo</i>

<sup>a</sup> Estimated from plate 1 (*a*) of the paper.

<sup>b</sup> Dorsal and abdominal  $D_{MRC}$ , respectively.

<sup>c</sup> Abdominal and dorsal  $D_{MRC}$ , respectively.

<sup>d</sup> Total range observed.

conditions. Kristensen (1981) studied the Cl<sup>-</sup> efflux in the short-circuited frog skin in the presence of, respectively, BIG (benzimidazolylguanidine) and AVT (arginine vasotocin) which both are known to activate the Na<sup>+</sup> permeability (Ussing & Zerahn, 1951; Fuchs et al., 1977; Nagel, 1978; Li et al., 1982). However, it was found that only BIG stimulates the Cl<sup>-</sup> flux. As the principal cells are AVT sensitive (Nagel, 1978), Kristensen concluded that the Cl<sup>-</sup> ions pass a BIG-sensitive, Na<sup>+</sup>-transporting cellular pathway which is parallel to the principal cells, and he suggested that these cells are the mitochondria-rich cells.

Voûte & Meier (1978) studied the Cl<sup>-</sup> influxes in frog skins exposed to Cl<sup>-</sup>-free Ringer's on the inside. The active Na<sup>+</sup> transport was eliminated with either amiloride or KCl Ringer's on the outside. Under these conditions it was found that the Cl<sup>-</sup> current was proportional to the number of m.r. cells per mm of sections of 1- $\mu\text{m}$  thickness. Furthermore, these investigators found that the m.r. cells, but not the principal cells, swelled following exposure of the skin to K-gluconate on the inside and KCl on the outside indicating that the apical membrane of the m.r. cells, only, is permeable to Cl<sup>-</sup>.

The results of the present study show that the Cl<sup>-</sup> current through the fully activated Cl<sup>-</sup> conductance (measured at  $V = -100$  mV) is linearly correlated to the density of m.r. cells (Fig. 12). The relation between  $D_{MRC}$  and  $I_{Cl}$  was found to be  $I_{Cl} = -2.6 \times 10^{-3} D_{MRC} + 11.6$ .  $D_{MRC}$  is a highly variable parameter, as seen from Table 7, which quotes some values from the literature. It is seen that  $D_{MRC}$  varies among individuals of the same species, as well as among different species. Also, it is apparent that  $D_{MRC}$  varies between different skin areas of a single animal, for instance between dorsal and abdominal skin areas. Further, recently  $D_{MRC}$  has been shown to be dependent on the salinity to which the animal has been adapted (Katz & Larsen, 1984).

Due to the small contribution of the m.r. cells to the total epithelial surface and the large observed  $I_{Cl}$  through the maximally activated Cl<sup>-</sup> conductance, our results indicate that the apical membranes of the m.r. cells possess a very high passive Cl<sup>-</sup> conductance. Considering a mean  $I_{Cl}$  per m.r. cell of  $-2.6$  nA (the slope of the observed relation between  $I_{Cl}$  and  $D_{MRC}$ ) we arrive at a conductance of about 200 mS per cm<sup>2</sup> surface area of mitochondria-rich cell. This impressive figure compares with the Cl<sup>-</sup> conductance of 580 mS/cm<sup>2</sup> of the Cl<sup>-</sup> cells of teleosts (Foskett et al., 1983) and with the peak Na<sup>+</sup> conductance of about 750 mS/cm<sup>2</sup> at the node of frog myelinated axon (Hille, 1984). However, due to the presence of microvilli (Whitear, 1975) on the apical membrane, the specific conductance of the apical membrane of m.r. cells might be an order of magnitude lower.

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